

REVIEW OF APPLIED MATHEMATICAL MODELS FOR DESCRIBING THE BEHAVIOUR OF AQUEOUS HUMOR IN EYE STRUCTURES

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In the paper, currently used methods for modeling the flow of the aqueous humor through eye structures are presented. Then a computational model based on rheological models of Newtonian and non-Newtonian fluids is proposed. The proposed model may be used for modeling the flow of the aqueous humor through the trabecular meshwork. The trabecular meshwork is modeled as an array of rectilinear parallel capillary tubes. The flow of Newtonian and non-Newtonian fluids is considered. As a results of discussion mathematical equations of permeability of porous media and velocity of fluid flow through porous media have been received.

Key words: porous medium, Newtonian fluid, non-Newtonian fluid, couple stress fluid, generalized second grade fluid, Darcy's rule, aqueous humor flow, trabecular meshwork, intraocular pressure, glaucoma.

1. Introduction

The aqueous humor is a substance responsible for keeping proper tension of the eyeball and for nutrition and purification of its structure. The correct value of intraocular pressure occurs when the aqueous humor is produced and drained into the ciliary body at the same rate the (Fig.1). As results of disorder of this process optic nerve can be damaged. Damage of the optic nerve causes permanent and total blindness. The value of intraocular pressure at 21 mmHg , considered as the highest acceptable value for healthy eye, was established (Nizankowska, 2006). A better understanding of pathomechanisms of diseases is the key to their effective treatment. Therefore it is very important to understand and describe the aqueous humor behavior in eye structures (Nizankowska, 2006).

In the literature a lot of mathematical models describing the behavior of the aqueous humor in the eye structures have been presented. All of them have in common the assignment of rheological properties of water to the aqueous humor. This is far-reaching simplification, because in aqueous collagen fibers, ascorbid acid and ions of various elements humor are suspended. Therefore the aqueous humor should be treated as a couple stress fluid, or power series fluid (Walicka and Walicki, 1999).

The aqueous humor consists of 98% water. The composition of the aqueous humor is approximate to blood plasma composition. Differences of quantity in percents of suspended elements between that two fluids are very small. Therefore, a considerable approximation of the aqueous humor properties would be determine the rheological properties of blood plasma. Blood donation is a much less invasive procedure than aqueous humor donation. Blood donation procedure is also much less risky (Gabelt and Kaufman, 1995; Gedde, 2012).

Discussion on the flow of the aqueous humor in eye structures and its meaning for the control of intraocular pressure was initiated by Goldman. In 1950 he developed a technique for monitoring the direction of the flow and for making a quantitative analysis of the flow. Goldman assumed that the method of administration and sampling the dye did not affect the test results, and defined - from post-injection of the dye (fluorescein) into

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the structures of the eye dye – the velocity and flow directions of the fluid. The test method proposed by Goldman was very invasive, because the dye was administered directly by injection into the eyeball.

Currently used methods of flow testing are less invasive and based on fluorophotometry. The dye is administered in the form of drops (Millar *et al.*, 2011).

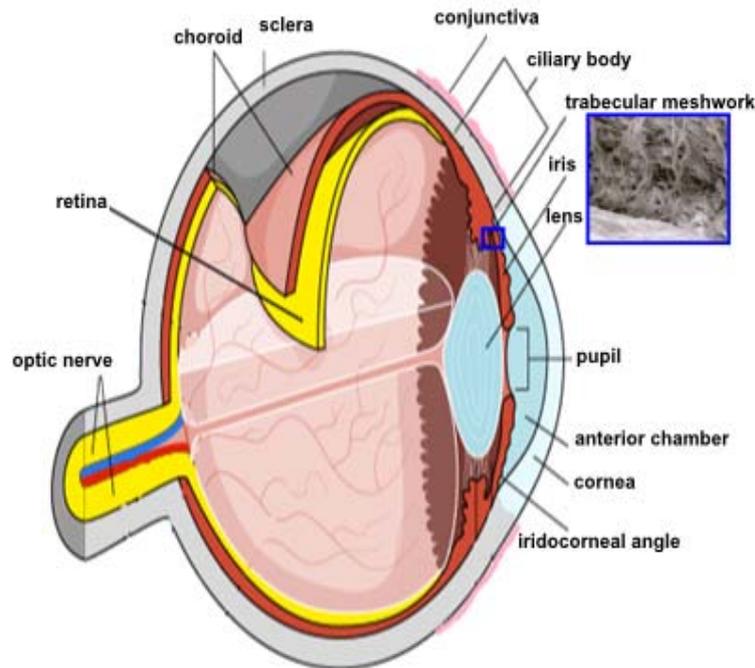


Fig. 1. The structure of the eyeball.

Another group of studies are the studies that describe the physical properties of the aqueous humor and specify the flow rate produced in the ciliary body. These studies determine the effect of the amount of the fluid produced, and the pressure in the blood vessels of the IOP. Based on experimental methods methods of mathematical description of the behavior of the aqueous humor in the eye structures have been developed. These phenomena were mathematically described by Friedland (Heys *et al.*, 2002). The model assumes a significant simplification, it is assumed that the tissues in the eye are rigid and do not affect the flow of the liquid. The geometry of the eye has also been simplified to the extent that it was possible to apply the Navier Stokes equations for the front and rear chamber. Friedland's model was developed by Tiedman (Heys *et al.*, 2002). He introduced an iris as diaphragm pressure relief valve. He assumed that it is supported on the edges and bears pressure on the inner surface. He simplified the model assuming an infinitely small thickness of the iris and the lack of its effect on the flow of the aqueous humor. Heys's model constitutes a development of the two previous solutions and considers the effect of the iris of a finite thickness for the flow of the aqueous humor (Heys *et al.*, 2002). Kaufman made certain assumptions about the passivity of the flow of the aqueous humor and its independence from energy. Moreover, he assumed that the outflow occurs only through the trabecular meshwork (Millar *et al.*, 2011). The flow of the aqueous humor in the anterior chamber of the eye was analyzed by Fitt and Gonzalez (2006). All the models presented above and used to describe the behavior of the fluid within the eye have one common feature, namely the assumption that the rheological properties of the aqueous fluid are comparable to the properties of water.

The objective of this paper is to analyze the possibilities of using rheological models of Newtonian and non-Newtonian fluids for mathematical modeling of the aqueous humor flow in the trabecular meshwork. The trabecular meshwork is modeled as a porous medium, which is a rectilinear array of parallel capillary tubes. A Newtonian fluid, a couple stress fluid and a generalized second grade fluid of a Shulman's type were considered as examples.

2. Mathematical models of the aqueous humor flow

2.1. Kaufman's model

The behaviour of the aqueous humor in the eyeball according to Kaufman and coworkers (Gabelt and Kauffman, 1995; Millar *et al.*, 2011) can be presented by the following equations

$$\begin{aligned} F_i &= F_s + F_f, \\ F_o &= F_t + F_u, \\ C_{tot} &= C_{trab} + C_u + C_{ps}, \\ F &= F_i = F_o \end{aligned} \tag{2.1}$$

where : F – the flow rate, F_i – the total flow of the aqueous humor to the eye, F_s – the flow of the aqueous humor through active secretion, F_f – the flow of the aqueous humor by filtration, F_o – the total outflow of the aqueous humor from the eye, F_t – the outflow of the aqueous humor through the trabecular meshwork, F_u – the outflow of the aqueous humor through the sclera, C_{tot} , C_{pp} – total conductance of the flow, C_{trab} , C_{TM} – conductance of the flow through the trabecular mesh, C_u – conductance of the flow through the sclera, C_{ps} – conductance of inflow of the aqueous humor.

The flow of the aqueous humor in the eye may be presented by the hydraulic model and Goldman's equation, assuming that the liquid flow is passive, an energy-independent and occurs in the direction of the pressure gradient. In addition, it is assumed that the outflow occurs only through the trabecular meshwork. This simplification shall be allowed, because 90% of the aqueous humor flows in this way. It can then be assumed that Eqs (2.2) and (2.3) determining the pressure difference Δp are true (Millar *et al.*, 2011)

$$\Delta p = p_i - p_v, \tag{2.2}$$

and the flow rate F

$$F = C_{trab}(p_i - p_v) \tag{2.3}$$

where p_i – the intraocular pressure, p_v – the episcleral vessels pressure.

For a human body the flow rate F amounts to

$$F = 0.28 \left[\frac{\mu\text{l}}{\text{min}} \right] (15.6 [\text{mmHg}] - 7.6 [\text{mmHg}]) = 2.24 \left[\frac{\mu\text{l}}{\text{min}} \right].$$

2.2. Heys's model

Heys's model (Heys *et al.*, 2002) assumes that the aqueous humor has the following properties: density $1000 \left[\frac{\text{kg}}{\text{m}^3} \right]$, viscosity $7.5 \cdot 10^{-4} \left[\frac{\text{kg}}{\text{ms}} \right]$ for $37[^\circ\text{C}]$, the Reynolds constant of 0.001 was determined for the flow in the eyeball by Friedman. The length scale of the flow of the aqueous humor was

$5 \cdot 10^{-4} [m]$, and the characteristic velocity of the flow was $2 \cdot 10^{-6} \left[\frac{m}{s} \right]$. Heys's model did not consider the dependence between the flow rate and intraocular pressure, his model also ignored the effects of the mass forces (Heys *et al.*, 2002). Equations determining the motion of a viscous liquid can be presented as

$$\begin{aligned} \nabla \underline{v} &= 0, \\ \rho \frac{d\underline{v}}{dt} &= -\nabla P + \mu \nabla^2 \underline{v}, \end{aligned} \quad (2.4)$$

leaving aside in Eqs (2.4) the effect of inertial forces we obtain (Heys *et al.*, 2002)

$$\begin{aligned} \nabla \underline{u} &= 0, \\ -\nabla P + G \nabla^2 \underline{u} &= 0. \end{aligned} \quad (2.5)$$

The geometrical dimensions of the eye in the model were taken from ultrasound and biomicroscopic examinations. The model takes into account the phenomenon of changing the shape of the iris and blinking. The eye model was created and analyzed using the finite element method in the software module FIDAP FIGEN. Heys gave the dependence that determines the flow of the aqueous humor within the eye of additional parameters (2.6), and a simplified version (2.7) (Heys *et al.*, 2002)

$$v_n = \frac{C_{TM} (p_o - p_v) + F_U}{A_o}, \quad (2.6)$$

$$v_n = \frac{C_{PP} (p_o - p_v)}{A_v} \quad (2.7)$$

where p_o – the pressure measured at the outlet of the trabecular meshwork, p_v – the episcleral vessels pressure.

The simplified version excludes the impact from drainage of the aqueous humor through the sclera (F_U) for a normal flow rate of fluid (v_n). It was assumed that the aqueous humor flows only through the trabecular network and therefore the conductance of the flow through the structure (C_{TM}) was replaced by the total conductance (C_{PP}). The flow area of the trabecular meshwork (A_o) was replaced by the total contact surface of the vitreous and aqueous humor (A_v).

2.3. Fitt's-Gonzalez's model

Fitt and Gonzalez (2006) analyzed the flow of fluid for five different groups of factors forcing the flow.

The factors were divided into groups associated with:

- fluctuations of temperature between individual structures of the eye.
- the production of the aqueous humor in the ciliary body,
- changes in eye position,
- effects of accommodation,
- eye movements during REM sleep.

They developed equations that describe the flow of the aqueous humor in the eye structures, by using the finite element method implemented in Femlab software (Fitt and Gonzalez, 2006)

$$-\frac{P_x}{\rho_0} + vu_{zz} + g[1 - \alpha(T - T_0)] = 0, \tag{2.8}$$

$$-\frac{P_y}{\rho_0} + v v_{zz} = 0, \tag{2.9}$$

$$p_z = 0, \tag{2.10}$$

$$u_x + v_y + w_z = 0, \tag{2.11}$$

$$T_{zz} = 0. \tag{2.12}$$

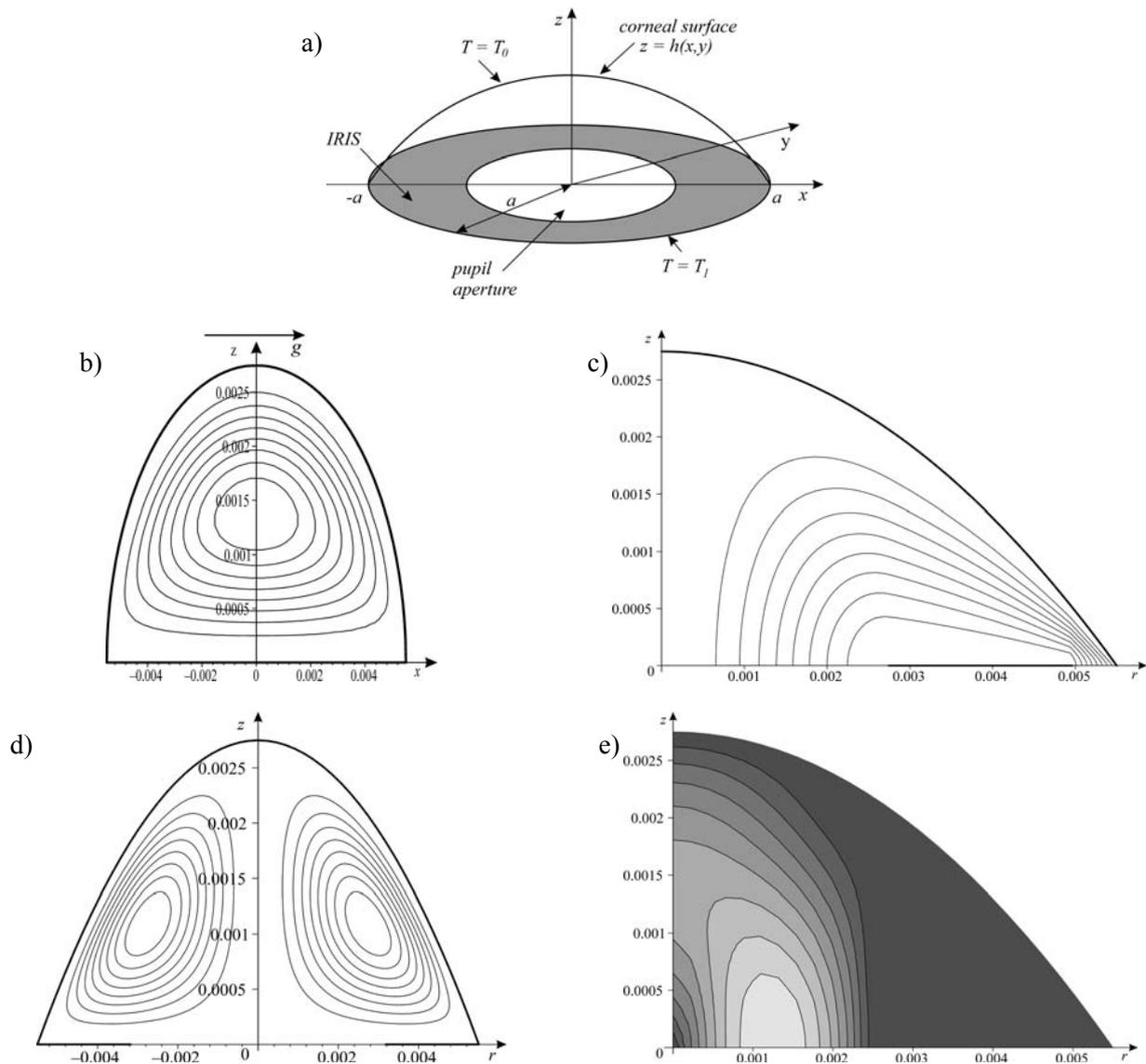


Fig.2. Aqueous humor flow in Fitt's-Gonzalez's model: a) boundary conditions, b) flow forced by temperature differences, c) flow forced by production of the aqueous humor by the ciliary body, d) flow during sleep, e) flow forced by eyeball movements (Fitt and Gonzalez , 2006).

The problem was analyzed considering the following boundary conditions

$$u = v = 0, \quad w = w_0(x, t), \quad T = T_l \quad \text{dla} \quad z = 0, \quad (2.13)$$

$$u = v = w = 0, \quad T = T_0 \quad \text{dla} \quad z = h(x, y). \quad (2.14)$$

Assuming the simplest case (i.e., no transfer through the aperture of the pupil ($w_0=0$), the gravity acting along the positive axis, and hydrostatic pressure), we determine $v=0$, therefore the flow is in a vertical plane (x, z) of the front chamber. The solution for this case is given by the following relationships

$$p = p_a + \frac{g\rho_0(x+a)(2-\alpha(T_l-T_0))}{2}, \quad (2.15)$$

$$T = T_l + \frac{z(T_0-T_l)}{h}, \quad (2.16)$$

$$\psi = -\frac{(T_l-T_0)gaz^2(z-h)^2}{24\nu h}. \quad (2.17)$$

In Eqs (2.8)-(2.17) fluid velocity is determined by $\mathbf{q} = (u, v, w)$, the coordinate system is shown in Fig.2, where p means the pressure, p_a – environmental pressure, g – acceleration due to gravity, a – the radius of the eyeball, ρ_0 – density, α – the coefficient of linear expansion, T – temperature, T_0, T_l – the temperature of the front and rear part of the cornea, ν – kinematic viscosity, ψ – current function.

Based on the analysis of the results obtained it was found that a temperature difference between the eye structures has the greatest impact on the circulation of the fluid in the structures of the eye. The velocity of the aqueous humor thus obtained is an order of magnitude greater than the flow rate enforced by other factors.

3. The proposed computational models for the flow of the aqueous humor through the trabecular meshwork

Most of the aqueous humor is drained from the eye to the ciliary body through the trabecular meshwork. In this way, about 90% of the aqueous humor is discharged. That is why it is necessary to develop computational models allowing a description of the behavior of biological fluids in the tissues. To approximate the behavior of the fluid within the trabecular network a model of a porous medium can be used, which consists of an array of parallel and straight glass capillary tubes, arranged parallel to the direction of the flow. In contrast, in mathematical modeling of the aqueous humor models of a Newtonian fluid, a couple-stress fluid and Shulman's fluid can be used.

3.1. Flow of a Newtonian fluid through a porous medium

The generalized model of a Newtonian fluid flow in porous media - obtained from Navier and Stokes - is known in the literature as a Brinkman-Forchheimer-Darcy model (Amiri and Vafai, 1994; 1998; Nakayama *et al.*, 2004; 2006). The equation of motion for this model can be represented by the following relationships (Walicka, 2002; Walicka and Walicki, 2012):

- continuity equation

$$\nabla \bar{\mathbf{v}} = 0, \tag{3.1}$$

- momentum equation

$$\frac{\rho}{\varphi_p} \left[\frac{\partial \bar{\mathbf{v}}}{\partial t} + (\bar{\mathbf{v}} \nabla) \bar{\mathbf{v}} \right] = -\nabla p + \frac{\mu}{\varphi_p} \nabla^2 \bar{\mathbf{v}} - \frac{\mu}{\Phi_n} \bar{\mathbf{v}} - \frac{\rho \mathbf{F} \varphi_p}{\sqrt{\Phi_n}} |\bar{\mathbf{v}}| \bar{\mathbf{v}} \tag{3.2}$$

where φ_p is the medium porosity, Φ_n – permeability, μ – dynamic viscosity, \mathbf{F} – geometric tensor, $\bar{\mathbf{v}}$ – averaged velocity, \bar{p} – averaged pressure.

Consider a Newtonian fluid in a porous layer having a thickness H_p , shown in Fig.3, which is a matrix composed of parallel rectilinear tubes. The flow rate of a Newtonian fluid in that layer - in accordance with Darcy’s law - is equal to Walicka (2002)

$$\bar{\mathbf{v}} = -\frac{\Phi_n}{\mu} \frac{d\bar{p}}{dy} \tag{3.3}$$

where Φ_n is permeability of the porous layer.

The flow rate of a Newtonian fluid in the capillary tube having a radius r_c (Fig.3) is given by the equation (Walicka, 2012)

$$v_y = \left(1 - \frac{r^2}{r_c^2} \right) \left(-\frac{d\bar{p}}{dy} \right), \tag{3.4}$$

and the flow rate \bar{Q} is determined by the equation

$$\bar{Q} = 2\pi \int_0^{r_c} v_y r dr . \tag{3.5}$$

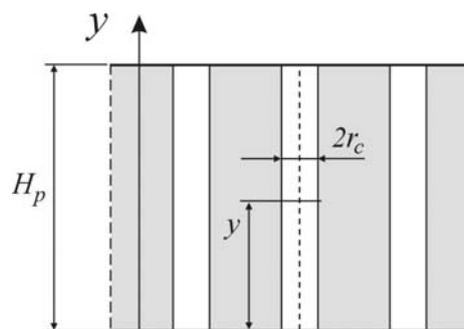


Fig.3. Porous area composed of parallel rectilinear tubes.

Finally, the Newtonian fluid flow rate in the capillary tube - basing on formulas (3.4) and (3.5) - is given by the equation

$$\bar{Q} = 2\pi \int_0^{r_c} \left(1 - \frac{r^2}{r_c^2}\right) \left(-\frac{d\bar{p}}{dy}\right) r dy = -\frac{\pi r_c^4}{8\mu} \frac{d\bar{p}}{dy}, \quad (3.6)$$

and averaged velocity in the capillary tube is equal to

$$\bar{v}_a = \frac{\bar{Q}}{\pi r_c^2} = -\frac{r_c^2}{8\mu} \frac{d\bar{p}}{dy}. \quad (3.7)$$

Taking into account the porosity of the medium consisting of capillary tubes

$$\Phi_p = \frac{N_c \pi r_c^2 H_p}{A H_p} = \frac{N_c \pi r_c^2}{A} \quad (3.8)$$

where N_c is the number of capillary tubes on the surface A of the porous medium, we obtain

$$\bar{v} = \bar{v}_a \Phi_p = -\frac{r_c^2 \Phi_p}{8\mu} \frac{d\bar{p}}{dy}. \quad (3.9)$$

Comparing Eqs (3.3) and (3.9), we get (Walicka, 2002; 2012; Walicka and Walicki, 2012)

$$\Phi_n = \frac{r_c^2 \Phi_p}{8}, \quad (3.10)$$

the equation determining permeability of the porous medium for a Newtonian fluid.

3.2. Flow of couple-stress fluid

Flows of couple-stress fluids were investigated first by Stokes (1966) and other subsequent researchers.

Considering the analysis presented in the papers (Walicka, 2002; 2012; Walicka and Walicki, 1999; 2012) equations of motion of couple-stress fluids may be presented in the following form

$$\operatorname{div} \mathbf{v} = 0, \quad (3.11)$$

$$\rho \frac{d\mathbf{v}}{dt} = \rho \mathbf{f} + \rho \frac{l}{2} \operatorname{curl} \mathbf{l} - \operatorname{grad} p + \mu \nabla^2 \mathbf{v} - \eta \nabla^4 \mathbf{v}, \quad (3.12)$$

$$\rho \frac{d\mathbf{e}}{dt} = \operatorname{div}(\lambda \operatorname{grad} T) + 2\mu \mathbf{D} : \mathbf{D} + 4\eta \mathbf{K} : \mathbf{K}, \quad (3.13)$$

$$\mathbf{K} = (\operatorname{grad} \boldsymbol{\omega})^T, \quad \boldsymbol{\omega} = \frac{l}{2} \operatorname{curl} \mathbf{v}. \quad (3.14)$$

In the theory of couple-stress fluids two tensors exist:

- the stress tensor

$$\mathbf{T} = -p\mathbf{I} + 2\mu\mathbf{D} - 2\eta\nabla^2\mathbf{W} \tag{3.15}$$

where \mathbf{D} is a symmetric grad \mathbf{v} and \mathbf{W} is an asymmetric part of the tensor

$$\mathbf{D} = \frac{1}{2}(\mathbf{L} + \mathbf{L}^T) = \frac{1}{2}(\nabla\mathbf{v} + \nabla\mathbf{v}^T), \quad \mathbf{D} = \mathbf{D}^T, \tag{3.16}$$

$$\mathbf{W} = \frac{1}{2}(\mathbf{L} - \mathbf{L}^T) = \frac{1}{2}(\nabla\mathbf{v} - \nabla\mathbf{v}^T), \quad \mathbf{W} = -\mathbf{W}^T,$$

\mathbf{D} is the deformation rate tensor, \mathbf{W} is the spin tensor, symbol T is the tensor matrix transposition

$$\text{grad } \mathbf{v} = \nabla\mathbf{v}; \tag{3.17}$$

- the couple-stress tensor

$$\mathbf{M}_s = 4\eta\mathbf{K} + 4\eta'\mathbf{K}^T \tag{3.18}$$

where η and η' are material constants associated with couple-stress.

Consider the flow of a couple-stress fluid through the capillary having a radius r_c , as shown in Fig.4. The axis y is the axis of symmetry of the tube. The velocity field is described by the equation

$$v_y = \left\{ I - \frac{r^2}{r_c^2} - \frac{2(\eta - \eta') \left[I_0\left(\frac{r_c}{l}\right) - I_0\left(\frac{r}{l}\right) \right]}{\frac{r_c}{l} \left[\eta \frac{r_c}{l} I_0\left(\frac{r_c}{l}\right) - (\eta + \eta') I_1\left(\frac{r_c}{l}\right) \right]} \right\} \frac{r_c^2}{4\mu} \left(-\frac{d\bar{p}}{dy} \right) \tag{3.19}$$

where $I_0(\rho)$ and $I_1(\rho)$ are the modified Bessel functions of the zeroth and the first order and the first kind.

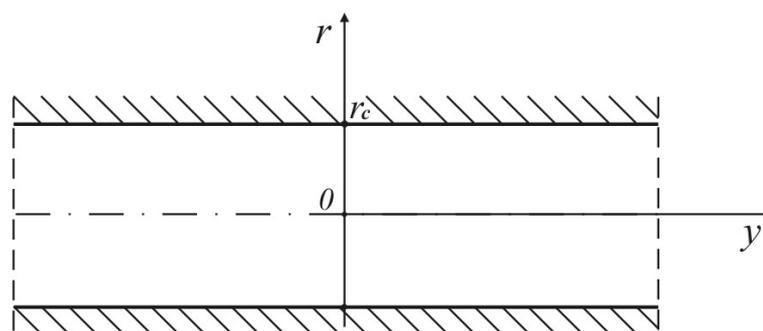


Fig.4. The geometry of the capillary tube.

The flow rate \bar{Q} is defined by Eq.(3.5). Substituting Eq.(3.19) into Eq.(3.5), we get

$$\bar{Q} = \frac{\pi r_c^4 \Phi_I(\Psi)}{8\mu} \left(-\frac{d\bar{p}}{dy} \right) \quad (3.20)$$

where

$$\Phi_I(\Psi) = I - \frac{4(\eta - \eta')}{N(\Psi)} \left[I_0(\Psi) - \frac{2}{\Psi} I_1(\Psi) \right], \quad \Psi = \frac{r_c}{l} \approx I, \quad (3.21)$$

$$N(\Psi) = \Psi \left[\eta \Psi I_0(\Psi) - (\eta + \eta') I_1(\Psi) \right], \quad I^2 = \frac{\eta}{\mu}.$$

Then we obtain

$$\bar{v}_a = \frac{\bar{Q}}{\pi r_c^2} = \frac{r_c^2}{8\mu} \Phi_I(\Psi) \left(-\frac{d\bar{p}}{dy} \right), \quad \text{for } \eta = \eta' \quad \Phi_I = I - \beta_c; \quad \beta_c = 8(\eta - \eta')^2, \quad (3.22)$$

and

$$\Phi_c = \frac{r_c^2 \Phi_p}{8} \Phi_I(\Psi), \quad (3.23)$$

Is the equation describing permeability of a couple-stress fluid.

3.3. Flow of generalized second grade fluids

Man and Sun (1987) and Tsai *et al.* (1988) were the first who presented the results of research on the flow of generalized second grade fluids. Results of research on the flow of the aforementioned fluids can also be found in the papers by Walicki and Walicka (Walicka 2002a; 2002b; Walicki and Walicka 1998; 1999; 2000a; 2000b; 2000c).

Motion equations of generalized second grade fluids can be presented in the form of

$$\text{div } \mathbf{v} = \theta, \quad (3.24)$$

$$\rho \frac{d\mathbf{v}}{dt} = \rho \mathbf{f} + \text{div } \mathbf{T} \quad (3.25)$$

where \mathbf{T} depends on the fluid model. Let us consider two models of fluids - proposed by Walickis (Walicki and Walicka, 1998) – based on the non-linear Shulman's model. Constitutive equations can then be presented as:

- model I

$$\mathbf{T} = -p\mathbf{I} + M\mathbf{A}_1 + \alpha_1 \mathbf{A}_1^2 + \beta_1 \mathbf{A}_2, \quad (3.26)$$

- model II

$$\mathbf{T} = -p\mathbf{I} + M \left(\mathbf{A}_1 + \alpha_2 \mathbf{A}_1^2 + \beta_2 \mathbf{A}_2 \right) \quad (3.27)$$

where

$$M = \left[\frac{1}{\tau_0^n} + (\mu A)_m \frac{1}{m} \right]^n A^{-1}, \quad A = \left[\frac{1}{2} \text{tr}(A_I^2) \right]^{\frac{1}{2}} \tag{3.28}$$

where A_I and A_2 are first two Rivlin's-Ericksen's tensors defined by the equations

$$A_I = 2D = (\nabla v + \nabla v^T), \quad A_2 = \dot{A}_I + A_I \nabla v + \nabla v^T A_I. \tag{3.29}$$

Consider the steady laminar flow of a generalized second grade fluid in the capillary tube having a radius r_c (Fig.5).

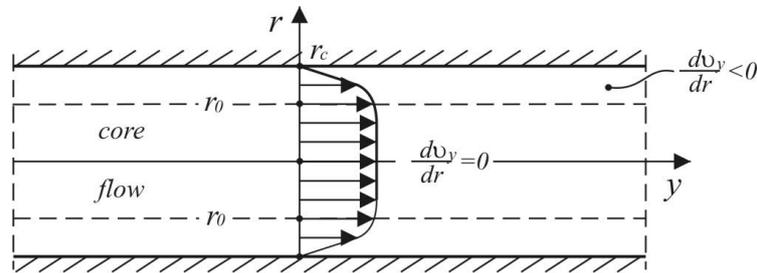


Fig.5. The coordinate system and velocity field in the capillary tube.

The velocity field is defined as follows:

– for shear flow

$$v_{ys}(r) = \frac{r_0}{\mu} \left(\frac{r_0 \tau_0}{r_c} \right)^{\frac{m}{n}} Y^{\frac{m}{n}} \sum_{i=0}^m \Phi_i \left[1 - \left(\frac{r}{r_c} \right)^{\frac{m+n-i}{n}} \right], \tag{3.30}$$

– for core flow

$$v_{yc} = v_{ys}(r_0); \tag{3.31}$$

where

$$\Phi_i = (-1)^i \frac{n}{m+n-i} C_m^i Y^{\frac{m+n-i}{n}} \quad \text{and} \quad Y = -\frac{r_c}{2\tau_0} \frac{\partial \bar{p}}{\partial y}. \tag{3.32}$$

The flow rate \bar{Q} is given by the equation

$$\bar{Q} = 2\pi \int_0^{r_c} v_y r dr = 2\pi \left[\int_0^{r_0} v_{yc} r dr + \int_{r_0}^{r_c} v_{ys} r dr \right]. \quad (3.33)$$

Using Eqs (3.32) and (3.33), we obtain

$$\bar{Q} = \frac{\pi r_c^3 \tau_0^m}{\mu} Y^{-3} \sum_{i=0}^m (-1)^i \frac{n}{m+3n-i} C_m^i \left[Y \frac{m+3n-i}{n} - 1 \right]. \quad (3.34)$$

Consider at the beginning the flow of a generalized second grade fluid of a power-law type in porous media consisting of a parallel system of straight capillaries. Equation (3.34) describes the flow rate in the capillary tube

$$\bar{Q} = \frac{\pi r_c^{m+3}}{2^m (m+3) \mu} \left(-\frac{d\bar{p}}{dy} \right)^m, \quad (3.35)$$

while the average speed in the capillary tube is given as follows

$$\bar{v}_a = \frac{\bar{Q}}{\pi r_c^2} = \frac{r_c^{m+3}}{2^m (m+3) \mu} \left(-\frac{d\bar{p}}{dy} \right)^m. \quad (3.36)$$

The analogue of Darcy's law can be represented by the equation

$$\bar{v} = \bar{v}_a \Phi_p = \frac{r_c^{m+3} \Phi_p}{2^m (m+3) \mu} \left(-\frac{d\bar{p}}{dy} \right)^m, \quad (3.37)$$

or

$$\bar{v} = -\frac{\Phi_p}{\mu} \left(-\frac{d\bar{p}}{dy} \right)^m, \quad \Phi_p = \frac{r_c^{m+3} \Phi_p}{2^m (m+3)}. \quad (3.38)$$

It can be noticed that the analogue of Darcy's law has the same form (independent of coefficients describing the viscoelastic properties of material α_i and β_i) for both models of generalized second grade fluid of a power-law type; the flow of Rivlin's-Ericksen's fluid (viscoelastic fluid) to the porous layer is defined by Darcy's law given by Eq.(3.3). Following in a similar way, an analogue of Darcy's law for any model of fluid can be designated.

Consider the flow of a Shulman's generalized second grade fluid of a power-law type in a porous medium consisting of a system of parallel, straight capillaries. Introducing the following equation

$$Y = \frac{r_0}{r_c}, \quad \tau_0 = \frac{r_c Y}{2} \left(-\frac{d\bar{p}}{dy} \right), \quad (3.39)$$

we obtain – considering Eqs (3.39) and (3.34) - equations for the Shulman's type fluid flow velocity through a porous layer. Results for selected empirical models of viscoplastic fluids are presented in Tab.1 (Walicka, 2012)

Table 1. The mathematical models of viscoplastic fluids (Walicka, 2002).

Model's inventor name	Mathematical Form	Designation	Equation no.
Bingham	$\tau = \tau_0 + \mu\dot{\gamma}$	τ - shear stress, τ_0 - yield point, $\dot{\gamma}$ - shear rate, μ - shear or plastic viscosity μ_0, μ_∞ - boundary viscosity m, n - exponents of the rheological equations of state κ - material constant	(3.40)
Herschel-Bulkley	$\tau = \tau_0 + (\mu\dot{\gamma})^{\frac{1}{m}}$		(3.41)
Vočadlo	$\tau = [\tau_0^{1/n} + \mu\dot{\gamma}]^n$		(3.42)
Casson	$\tau = [\tau_0^{1/n} + (\mu\dot{\gamma})^{1/n}]^n$		(3.43)
Shulman	$\tau = [\tau_0^{1/n} + (\mu\dot{\gamma})^{1/m}]^n$		(3.44)
Briant	$\tau = \mu \left(1 + \frac{\tau_\infty}{\kappa\mu\dot{\gamma}} \right)^m \dot{\gamma}$		(3.45)
Tscheuschner	$\tau = \left[\mu_\infty + \frac{\tau_0}{\dot{\gamma}} + \frac{\mu_0}{(\mu\dot{\gamma})^n} \right] \dot{\gamma}$		(3.46)

It may be noted that the simplification of Shulman's model coefficients leads to the formulas describing the flow curves for simpler models of fluids such as:

- Casson's model: $m = n$ and $m = n = 2$;
- Vočadlo's model: $m = 1$, $n \neq 0$;
- Herschel's-Bulkley's model: $m \neq 0$, $n = 1$;
- Bingham's model: $m = n = 1$;
- Ostwalda-de Wael's model: $n = 1$, $\tau_0 = 0$;
- Newton's model: $m = n = 1$, $\tau_0 = 0$.

4. Summary and conclusions

Despite the existence of many mathematical models describing the behavior of the aqueous humor in eye structures, which relatively well capture the essence of the phenomena in the eye, a common feature of these models should be noted; namely, the assignment of rheological properties of water to the aqueous humor. This simplification is probably due to the fact that the investigation of the rheological properties of the aqueous humor is impeded. Difficulties in the study of the rheological properties of the aqueous humor arise from the fact that it is a substance found in the body in very small quantities. In a normal eye there is only 3.000 [μ l]. The amount that can be taken without disruption of the eyeball functioning is very small. A considerable increase in the level of complexity of the analytical model when taking into account the rheological properties of the aqueous humor is also of significant importance. The increased complexity of the model will complicate the obtainment of analytical solutions.

It is also important that biological fluids under extracorporeal conditions are subject to rapid degradation. Along with the degradation of the material all its characteristics change. Hence it is necessary to set the measurement path near the place where test material is taken (Chotard-Ghodsniya and Verdier, 2007; Fauci and Gueron, 2001; Verdier *et al.*, 2009).

In the paper, a proposal to use rheological models of Newtonian and non-Newtonian fluids (Walicka, 2002; Walicka and Walicki, 2012) for mathematical modeling of the aqueous humor flow in the structures of the eye is presented. Equations for the permeability of the porous material and liquid flow velocity in a porous medium are given. The trabecular meshwork was modeled as a porous medium, which is a rectilinear array of parallel capillary tubes. A Newtonian fluid, a couple-stress fluid and a generalized second grade fluid of a Shulman's type were considered as examples.

Nomenclature

- A_o – surface of the trabecular meshwork - in human body about $18 [mm^2]$
- A_v – contact surface of the vitreous and aqueous humor- in human body about $65 [mm^2]$
- C_{ps} – flow conductance of the aqueous humor- in human body about $0.061-0.081 \left[\frac{\mu l}{mmHg \cdot min} \right]$
- C_{tot}, C_{pp} – total flow conductance $\left[\frac{\mu l}{mmHg \cdot min} \right] \left[\frac{\mu l}{Pa \cdot s} \right]$
- C_{trab}, C_{TM} – conductance flow through the trabecular meshwork - in human body about $0.28 \left[\frac{\mu l}{mmHg \cdot min} \right]$ or $3.8 \cdot 10^{-5} \left[\frac{\mu l}{Pa \cdot s} \right]$
- C_u – flow conductance through the sclera- in human body about $0.02 \left[\frac{\mu l}{mmHg \cdot min} \right]$
- F – geometric tensor
- F – flow rate $\left[\frac{\mu l}{min} \right]$
- F_f – flow of the aqueous humor by filtration - about $90\% F_{in} \left[\frac{\mu l}{min} \right]$
- F_i – total inflow of the aqueous humor to the eyeball, in human body about $2-2.5 \left[\frac{\mu l}{min} \right]$
- F_o – total outflow of the aqueous humor from the eyeball $\left[\frac{\mu l}{min} \right]$
- F_s – flow of the aqueous humor through active secretion- about $10\% F_{in} \left[\frac{\mu l}{min} \right]$
- F_t – outflow of the aqueous humor through the trabecular meshwork $\left[\frac{\mu l}{min} \right]$
- F_u –outflow of the aqueous humor through the sclera $6.7 \cdot 10^{-3} \left[\frac{\mu l}{s} \right]$ or $1.12 \cdot 10^{-4} \left[\frac{\mu l}{min} \right]$
- G – the shear modulus of the iris, set as $G = \frac{1}{3} E = 9 [kPa]$
- p – pressure $[mmHg]$
- p_e, p_v – episcleral vessels pressure - in human body about $7.6-11.6 [mmHg]$
- p_i, p, \bar{p} – intraocular pressure- in human body about $15.6 \pm 3.2 [mmHg]$

- p_o – pressure at the outlet of the trabecular meshwork [mmHg]
 R – flow resistance $\left[\frac{\text{mmHg} \cdot \mu\text{l}}{\text{min}} \right]$
 T, T_I, T_0 – temperature [$^{\circ}\text{K}$]
 u – displacement of the iris
 \underline{v}, \bar{v} – flow velocity
 v_n – normal flow velocity
 μ – dynamic viscosity
 $\bar{\mathbf{v}}$ – average velocity vector
 Φ_n – permeability
 ϕ_p – porosity
 ψ – current line

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